

Research Paper

Evans Blue Attachment Enhances Somatostatin Receptor Subtype-2 Imaging and Radiotherapy

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Abstract

Purpose: Radionuclide therapy directed against tumors that express somatostatin receptors (SSTRs) has proven effective for the treatment of advanced, low- to intermediate-grade neuroendocrine tumors in the clinic. In clinical usage, somatostatin peptide-based analogs, labeled with therapeutic radionuclides, provide an overall response rate of about 30%, despite the high cumulative activity injected per patient. We set out to improve the effectiveness of somatostatin radiotherapy by preparing a chemical analog that would clear more slowly through the urinary tract and, concomitantly, have increased blood circulation half-life and higher targeted accumulation in the tumors. **Experimental Design:** We conjugated a common, clinically-used SST peptide derivative, DOTA-octreotate, to an Evans blue analog (EB), which reversibly binds to circulating serum albumin. The resulting molecule was used to chelate ⁸⁶Y and ⁹⁰Y, a diagnostic and a therapeutic radionuclide, respectively. The imaging capabilities and the radiotherapeutic efficacy of the resulting radioligand was evaluated in HCT116/SSTR2, HCT116, and AR42J cell lines that express differing levels of SST2 receptors. **Results:** The synthesized radiopharmaceutical retained affinity and specificity to SSTR2. The new molecule also retained the high internalization rate of DOTA-octreotate, and therefore, showed significantly higher accumulation in SSTR2-positive tumors. Labeling of our novel EB-octreotate derivative with the therapeutic, pure beta emitter, ⁹⁰Y, resulted in improved tumor response and survival rates of mice bearing SSTR2 xenografts and had long term efficacy when compared to DOTA-octreotate itself. **Conclusions:** The coupling of a targeted peptide, a therapeutic radionuclide, and the EB-based albumin binding provides for effective treatment of SSTR2-containing tumors.

Key words: SSTR2, PET, peptide radiotherapy, Evans blue, albumin.

Introduction

Gastroenteropancreatic neuroendocrine tumors are low-incidence tumors that typically are well differentiated and slow growing, though some are quite aggressive (1). Most of these tumors are only discovered after metastatic spread where treatment is more difficult (2). They are often noted for the production and release of neuroamines and hormonal peptides depending on tumor origin, including serotonin, kinins, vasoactive peptides, corticotropic hormone, *etc.* (3). Nearly 80% of these tumors express somatostatin receptors (1). Treatment of patients,

especially those with carcinoid syndrome, with octreotide, a somatostatin ligand, is used clinically to ameliorate symptoms related to the excess hormonal production (1, 2, 4).

Somatostatin (SST) peptide hormone, originally isolated from the hypothalamus, is a growth hormone inhibitory substance. The peptide has two naturally occurring biologically active forms, SST14 and SST28; both act as inhibitors of exocrine, endocrine, paracrine and autocrine activity (5-7). SST is produced by endocrine-like cells mainly found in the nervous

systems, the endocrine pancreas, and the gastrointestinal system (5, 6). SST function is mediated specifically by five distinct subtypes of G-protein coupled receptors, namely somatostatin receptors 1–5 (SSTR1–5) (1, 7). These SSTRs are widely expressed in various tumors (8, 9).

SSTR2, the most ubiquitous and abundant subtype in tumor tissues, can activate or suppress various signal transduction pathways (2). Specific SSTR subtypes are expressed by a given tumor depending on tumor type, and some cancers were reported to lose or gain expression of SSTRs (1, 10, 11). For example, loss of the SSTR2 expression in some human adenocarcinomas was implicated in the loss of cell regulation and subsequent proliferation. Because the receptors have been lost, no SST targeted therapy is possible (12). Another layer of complexity observed in some tumors is that the SSTRs form both homo- and heterodimers on the membrane, which confer new and/or different functional features (1, 8, 10, 11, 13, 14).

Therapeutics directed primarily at SSTR2 and SSTR5 employ synthetic analogs of the rapidly degraded natural ligand. Hexapeptide and octapeptide SST analogs were developed that incorporate the biologically active core of SST14, possess superior metabolic stability, and have longer circulation half-life (1.5–2 h) compared to the natural SST (1, 2, 5–8). Preclinical studies with SST analogs showed antitumor and anti-secretory effects *in vitro* and *in vivo*; however, the clinical efficacy was relatively limited (8, 9). One approach to improve this therapy was to develop SSTR2-targeted peptide-receptor radionuclide therapy (PRRT) that takes advantage of the fact that SSTR2 binding leads to ligand internalization. The rapid internalization and accumulation of the radiopharmaceutical inside tumor cells in proximity to the nucleus resulted in radioactivity-induced cell death (1, 4). The PRRT ligand was prepared by conjugation of a metal-binding complex to the peptide and then chelation of high energy β -emitting isotopes such as ^{90}Y and ^{177}Lu . ^{90}Y is a pure beta-emitter with a half-life of 64.1 hours, maximum energy of 2.28 MeV, and penetration range of 11 mm. SSTR2-targeted PRRT has been used in the clinic for more than two decades as a treatment of neuroendocrine tumors (NETs). Several Phase I and II clinical trials showed favorable results in NETs in general and even better results in patients with gastroenteropancreatic neuroendocrine tumors (GEPNETs) and bronchial NETs, where as much as 30% objective response was observed (4).

The most frequently used somatostatin analogs in PRRT clinical practice are octreotide and octreotate (TATE); the latter one has higher affinity and

selectivity towards SSTR2. Both peptides were conjugated to the bifunctional chelator 1,4,7,10-tetraazacyclododecane-1,4,7,10-tetraacetic acid (DOTA) for chelation of either ^{177}Lu or ^{90}Y . Both peptides clear from the blood through the kidneys, which is the critical organ in terms of radiation toxicity, and limits maximum dosage such that exposure is in the range of 23 to 29 Gy (15–17). The toxicity to the bone marrow is usually mild and transient.

To improve the pharmacokinetics of SSTR2 analogs and reduce PRRT toxicity, we conjugated a truncated Evans Blue (EB) molecule onto octreotate (EB-TATE). The EB moiety provided reversible binding of EB-TATE to albumin *in vivo* to extend the half-life in the blood. When the EB-TATE was slowly released into the tumor microenvironment, tumor uptake and internalization into SSTR positive cells resulted in delivery of radioactive particles and tumor cell killing. EB-TATE displayed significantly more favorable pharmacokinetics than TATE by achieving higher tumor to non-tumor contrast for both diagnostic positron emission tomography (PET) imaging with ^{86}Y and radiotherapy using ^{90}Y .

Materials and Methods

Syntheses, radiosyntheses, purification methods, and characterization of TATE, EB-TATE, and radiolabeled analogs are described in the Supplementary Materials.

Cell culture

HCT116 (human colon cancer) and AR42J (Rat amphicrine pancreatic) cells were purchased from American Type Culture Collection (ATCC). HCT116/SSTR2⁺ transfected cells were kindly provided to us by Dr. Carolyn Anderson, University of Pittsburgh Cancer Institute. Cells were cultured in McCoy's 5A medium (Hyclone) containing 10% fetal bovine serum (Gibco) in a humidified atmosphere containing 5% CO₂ at 37 °C.

Immunofluorescence and flow cytometry

SSTR2 levels in all three cell lines were determined by flow cytometry and immunofluorescence. 10⁵ cells/well were seeded in either 8-well chamber slides (Lab-Tek, immunofluorescence) or 24-well plates (Corning, flow cytometry). The medium was removed and the cells were washed twice with phosphate buffered saline (PBS, 500 μL). Then bovine serum albumin (2% BSA, 500 μL) was added and the cells were incubated for 1 h at 4 °C, followed by addition of anti-SSTR2 monoclonal antibody or isotype control (R&D Systems, 1:100 dilution). The cells, with the antibody, were incubated for an additional 1 h at room

temperature followed by three PBS washes. Subsequently, goat anti-mouse antibody (R&D Systems, 500 μ L, 1:100 in 2% BSA) was added and the cells were incubated for additional 1 h at room temperature, followed by three PBS washes. Cells were mounted with UltraCruz mounting medium containing DAPI (Santa Cruz Biotechnology, TX) and fluorescence images were determined by an epifluorescence microscope (200 \times ; Olympus, X81) or a confocal microscope (ZEISS). For flow cytometry, the cells were quantitatively analyzed by LSR II (BD Biosciences) using FlowJo (Tristar).

Cell binding assay

10^5 HCT116/SSTR2 cells per well were seeded in a 96-well membrane plate (Whatman) with 7.4 KBq of ^{86}Y -TATE and increasing concentrations of TATE or EB-TATE peptides ranging from 0 - 5000 nM. After 1 h incubation, the plate was washed three times with PBS. Subsequently, the cells were assayed in a gamma-counter. Binding affinity was calculated using GraphPad Prism by nonlinear regression. Experiments were performed in triplicate.

Kinetic binding assay by biolayer interferometry (BLI)

Binding assay of EB-TATE to biotinylated BSA/streptavidin biosensors was performed by BLI using an Octet Red96 system (fortéBio) in black 96-well plates (Geiger Bio-One). The assay protocol was as follows: 1) baseline (1 \times PBS) 60 s; 2) loading (biotin-labeled BSA, 1 μ g/mL) 600 s; 3) baseline (1 \times PBS) 60 s; 4) quenching (1 μ g/mL Biotin (Thermo Scientific)) 180 s; 5) baseline (1 \times PBS) 60 s; 6) association 600 s; 7) dissociation 600 s. Nonspecific binding calculated from measuring binding of BSA-loaded biosensor to buffer alone and blank biosensor to analytes was subtracted from the binding values. Data collected was analyzed using Octet Analysis software 7.0.

Cell uptake/internalization

Twenty-four h before the assay, 10^5 cells/well were distributed into 24-wells plate. Cells were washed with PBS X3 and then 18.5 KBq/well of ^{86}Y -EB-TATE or ^{86}Y -TATE were added in 0.5 mL of medium containing 1% (w/v) human serum albumin (HSA). At each indicated time point, the cells were washed X2 with PBS and lysed with 0.1M NaOH. Internalization was measured after removal of membrane-bound tracer by 1 min incubation with 0.5 mL of acid buffer (50 mM glycine, 100 mM NaCl, pH 2.8), wash X2 and lysis. Radioactivity of cell lysate was measured by a γ -counter (Perkin Elmer). The cell uptake and internalization values were normalized as

a percent of added radioactivity. Each time point was measured in triplicate.

Mouse xenografts model

Animal protocols were approved by the NIH Clinical Center Animal Care and Use Committee (ACUC). Female athymic nude/nude mice (6-7 weeks, 20-23g) (Harlan) were inoculated on their right shoulder with 5×10^6 cells of either; HCT116/SSTR2⁺, HCT116 or AR42J cells in Matrigel (Sigma) 1:1.

In vivo PET and biodistribution studies

PET assays were performed at 25-28 days post tumor cells inoculation when the tumor volume reached about 200-350 mm³. Mice were injected intravenously with 0.92 MBq (4 nmol) of either ^{86}Y -EB-TATE (n = 6, HCT116/SSTR2⁺; n = 5, HCT116) or ^{86}Y -TATE (n = 4) and scanned for 10-20 min at 1, 4, 24 and 48 h post injection (p.i.). Blocking studies were performed by co-injection with 50-fold excess of unlabeled EB-TATE (n = 3). PET studies were acquired on Nanoscan PET/CT (Mediso) and Inveon (Siemens) scanners. Images were reconstructed using a 3D ordered subset expectation maximum algorithm, and ROI were drawn using IRW (Siemens) and VivoQuant (INVICRO). After the last scan at 48h time point, tumor, heart, lung, liver, spleen, stomach, intestine, pancreas, kidney, muscle, bone and blood were collected from euthanized mice, weighed and measured in a gamma counter. Results are normalized as percentages of the injected dose per gram of tissue (%ID/g).

Tumor radiotherapy studies

Tumor treatment studies were performed in three different cell lines to evaluate the therapeutic efficacy of intravenous injection/s of ^{90}Y -EB-TATE vs. saline and ^{90}Y -TATE in both SSTR2⁺ and SSTR2⁻ xenografts. The study was commenced 20 days post inoculation of HCT116/SSTR2⁺ and HCT116 (SSTR2⁻) xenografts, when all the mice had tumor volume of about 150 mm³. HCT116/SSTR2⁺ xenografts were divided into 5 groups as followed; 1) saline (n = 6), 2) 7.4 MBq ^{90}Y -EB-TATE (n = 9), 3) 7.4 MBq ^{90}Y -EB-TATE (n = 5) (one dose), 4) 3.7 MBq ^{90}Y -EB-TATE (n = 8), and 5) 7.4 MBq ^{90}Y -TATE (n = 5). HCT116 (SSTR2⁻) xenografts were divided into additional 2 groups; 6) saline (n=5) and 7) 7.4 MBq ^{90}Y -EB-TATE (n=6). All the mice received the first dose at day 20 (start of treatment). Excluding group 3, which received only one dose by design, animals in all the other groups in which the tumor volume had not exceeded the experimental endpoint, received an additional injection at day 48. All the living mice were monitored for 180 days.

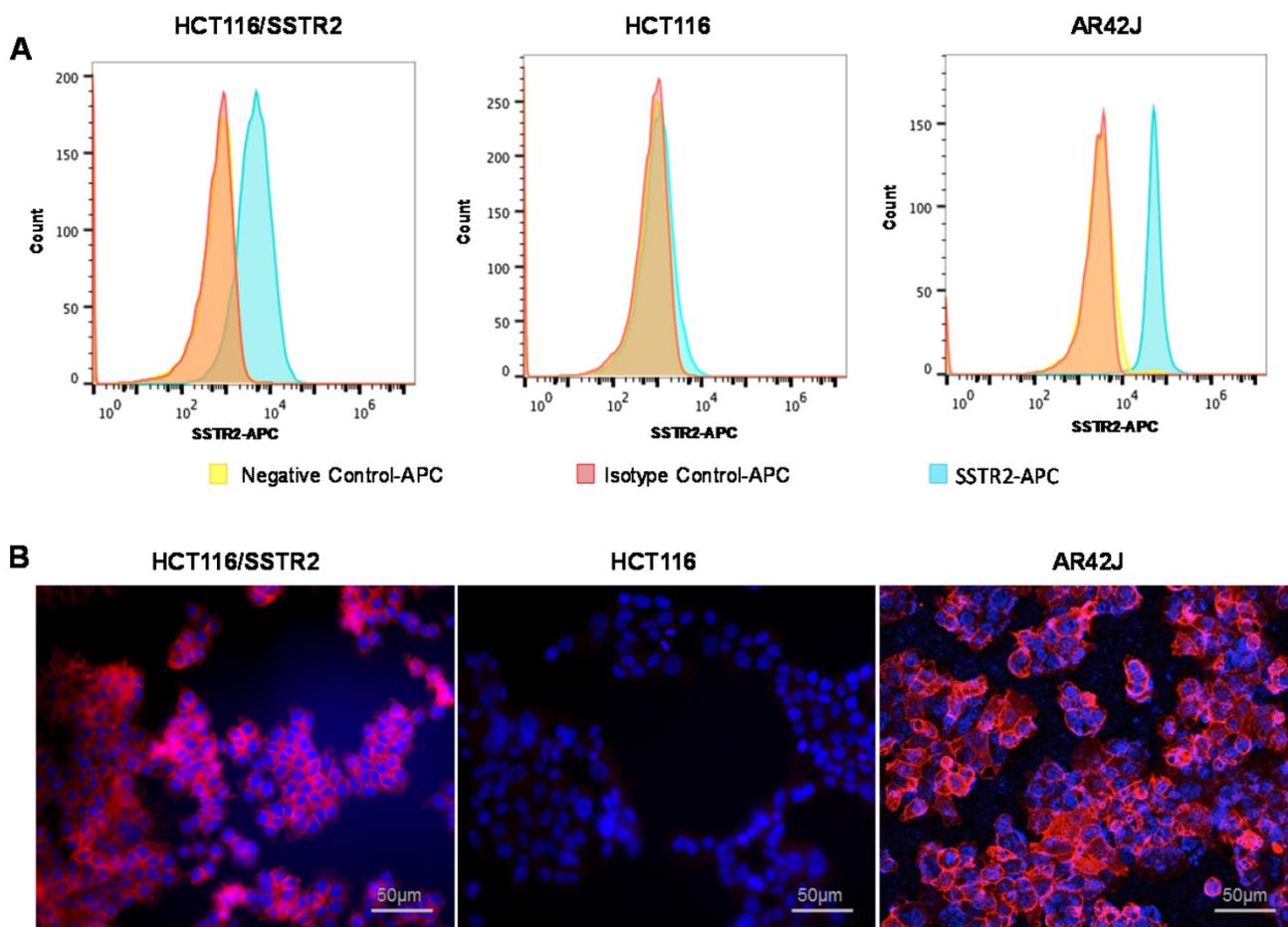


Figure 1. Evaluation of SSTR2 expression levels by cell lines. (A) Representative histograms of SSTR2 expression evaluated by flow cytometry showing unstained cells (negative control), an isotype control antibody and anti-SSTR2 antibody of HCT116 (low levels), HCT116/SSTR2 (medium levels) and AR42J (high levels). (B) Representative immunofluorescence staining (X20) of Anti-SSTR2 (red) and nucleus (DAPI, blue).

Another radiotherapy study was done in AR42J xenografts and started 15 days post-inoculation with tumor volumes at about 100 mm³. In this study, we had 4 groups; 1) saline (n = 3), 2) 7.4 MBq ⁹⁰Y-EB-TATE (n = 3), 3) 3.7 MBq ⁹⁰Y-EB-TATE (n = 3) and 4) 7.4 MBq ⁹⁰Y-TATE (n = 11). All the groups received only one radiotherapy dose at day 15. All the living mice were monitored for up to 90 days. Mice body weight and tumor volume were monitored every 2 days throughout the experiment. The formula used for calculation of tumor volume was $V = \text{width}^2 \times \text{length} / 2$.

Endpoint criteria defined by the institute ACUC was weight loss of more than 15%, a tumor volume > 1800 mm³, active ulceration of the tumor or abnormal behavior indicating pain or unease. These definitions were used for Kaplan-Meier analysis as well.

Histopathologic staining

Tumor tissues from each group described above were collected at different time points and frozen or kept at room temperature in Z-FIX (Anatec Ltd). 10 μm-thick sections were mounted on slides using a

cryo-microtome. Ki-67, TUNEL and H&E staining were done according to our previous work (18). Number of Ki67-positive nuclei was analyzed by visual counting on 5-6 fields of view per slide, 5 slides for each mouse and 3 mice per group. Quantification was done using Image J software (NIH).

Statistical Analysis

Unless described otherwise, results are mean ± SD. Two-tailed paired and unpaired Student's t tests were used to determine differences within groups and between groups, respectively. P values <0.05 were considered statistically significant.

Results

Cell characterizations and cell binding of EB-TATE

SSTR2 surface expression by HCT116/SSTR2 and AR42J was validated using Flow cytometry and compared to the parental cell line HCT116 that was SSTR2 negative (Fig. 1A). These results were also confirmed by immunofluorescence staining *in vitro*

and in tumor sections *ex vivo* (Fig. 1B and Supplementary Fig. S1). EB-TATE (Fig. 2A) was synthesized as described in the supplementary materials and was successfully labeled with Yttrium radioisotopes. The conjugation of TATE to truncated EB can affect the binding of each molecule to its target, therefore we tested the binding of EB-TATE to both SSTR2 and albumin *in vitro*. EB-TATE displayed similar binding characteristics to SSTR2 when compared to TATE alone (Fig 2B and Supplementary Fig. S2A), its binding affinity to serum albumin gave high association constant, K_{on} of 58233 and low dissociation constant, K_{off} of 0.2843 (Fig. 2C). EB-TATE affinity to serum albumin was in the range of μM (K_D of 4.8 μM) and IC_{50} of $1.92 \pm 0.34 \mu\text{M}$ (Supplementary Fig. S2C), which is comparable to the published binding affinity of Evans blue to albumin (19). To further ensure that the conjugation of EB to TATE does not reduce the peptide biological activity, we compared cell uptake and internalization studies *in vitro* in SSTR2 positive and negative cells between ^{86}Y -EB-TATE and ^{86}Y -TATE. Cell uptake of both tracers in HCT116/SSTR2 was similar at all time points and increased over time to reach values of $12.05 \pm 0.67\%$ and $10.38 \pm 1.82\%$, respectively, at 24 h. The uptake/internalization of both ^{86}Y -EB-TATE and ^{86}Y -TATE was significantly higher in SSTR2 positive than SSTR2 negative cells ($p < 0.001$, Fig. 2D and Supplementary Fig. S2B). Using excess amount of unlabeled EB-TATE and/or TATE reduced the uptake in SSTR2-positive cells to the low levels observed in SSTR2-negative cells ($p < 0.001$, Fig. 2D and Supplementary Fig. S2B). ^{86}Y -TATE and ^{86}Y -EB-TATE both internalized rapidly into SSTR2 positive cells in a comparable manner, confirming that EB conjugation did not reduce the biological activity of the peptide (Fig. 2D and Supplementary Fig. S2B).

^{86}Y Radiolabeled EB-TATE for tumor PET imaging

Next, we evaluated ^{86}Y -EB-TATE uptake *in vivo* in tumor xenografts and compared it to ^{86}Y -TATE (Fig. 3). ^{86}Y -EB-TATE uptake in SSTR2 positive tumors (HCT116/SSTR2) gradually increased over time. As designed, conjugation of TATE to EB increased its half-life in the blood when compared to ^{86}Y -TATE ($p < 0.001$, Figs. 3A and 3C). It is important to note that although the half-life in the blood was only increased by 2-fold, the amount of ^{86}Y -EB-TATE retained in the blood is 4-fold compared to ^{86}Y -TATE at 1 h and remained available for SSTR2 binding for longer time (Supplementary Fig. S3A). At 1 h p.i., most of ^{86}Y -EB-TATE was bound to serum albumin and the tracer was slowly released over time, the blood uptake decreased and tumor uptake increased

in SSTR2⁺ tumors but not in SSTR2⁻ tumors (Figs. 3A and 3C). At 24 h p.i., ^{86}Y -EB-TATE accumulated in the tumor to give high tumor-to-muscle and tumor-to-blood ratios (Fig. 3C). A representative co-registration of PET/CT at 24 h p.i. is shown in Fig. 3B. ^{86}Y -TATE on the other hand, showed a significantly less favorable pharmacokinetics, rapidly cleared through the urinary tract (Fig. 3A), with peak uptake in the tumor at 1 h p.i. and much lower accumulation in SSTR2⁺ tumors of about 5%ID/g (Figs. 3A and 3C). Biodistribution of the two tracers confirmed the PET studies showing a significantly higher tumor uptake of ^{86}Y -EB-TATE in comparison to ^{86}Y -TATE (Supplementary Fig. S3B).

^{86}Y -EB-TATE pharmacokinetics *in vivo* and specificity to SSTR2 was also evaluated in AR42J xenografts (Figs. 3D and 3E and Supplementary Fig. S4). Similar to the results observed in transfected HCT116/SSTR2 xenografts, ^{86}Y -EB-TATE at 1 h p.i. was mainly bound to serum albumin and circulated in the blood. ^{86}Y -EB-TATE was released from albumin over time and accumulated in the tumor, reaching high tumor uptake of $60.54 \pm 8.03 \text{ \%ID/g}$ ($p = 0.0067$), and $65.77 \pm 7.59 \text{ \%ID/g}$ ($p = 0.0059$) at 24 and 48 h p.i., respectively, and displayed high tumor-to-background ratios (Figs. 3D and 3E). ^{86}Y -EB-TATE accumulation in the tumor was efficiently blocked by co-injection of 50-fold excess of unlabeled EB-TATE (Figs. 3D and 3E and Supplementary Fig. S4), indicating that tumor accumulation was SSTR2 specific.

Radionuclide therapy of SSTR2⁺ tumors

The encouragingly high tumor uptake of ^{86}Y -EB-TATE, coupled with high internalization into the tumor cells resulted in high exposure to the radioactive isotope, as evident from area under the curve (AUC) calculation from non-decay corrected data (Supplementary Fig. S5). This led us to hypothesize that it would be an excellent SSTR2-targeted radiotherapy agent using the beta-emitting radionuclide ^{90}Y . Moreover, ^{86}Y -EB-TATE activity accumulated in the tumor, remained steady from 24 h time point (Fig. 3), suggesting a significantly higher tumor exposure from ^{90}Y than ^{86}Y because of the half-life difference of 64.1 h compared to 14.7h respectively. We tested the therapeutic efficacy in the three models that we had studied with imaging: HCT116/SSTR2 (medium SSTR2 level), HCT116 (SSTR2 negative) and AR42J (high SSTR2 level). Treatment with ^{90}Y -EB-TATE (3.7 and 7.4 MBq) had dramatic inhibitory growth effects on established tumors expressing SSTR2 such as HCT116/SSTR2 and AR42J. In both models, tumor volumes significantly decreased ($p < 0.001$) and mice

survival significantly extended ($p < 0.001$) when compared to saline and ^{90}Y -TATE groups or to injection of ^{90}Y -EB-TATE into HCT116 xenografts (Figs. 4A and 4B). ^{90}Y -EB-TATE exhibited dose dependency on both radioactivity amount as well as SSTR2 expression. Dosage dependency of ^{90}Y -EB-TATE was evident in the HCT116/SSTR2 tumor model, where the group which received 3.7 MBq had transient tumor regression for about two weeks post treatment, while an injection of 7.4 MBq displayed near-complete tumor regression (Fig. 4A and Supplementary Fig. S6). Unexpectedly, a second injection of ^{90}Y -EB-TATE to the 3.7 MBq group did not have any effect on tumor growth. To evaluate if the recurring tumors still express SSTR2, we imaged the mice with ^{68}Ga -DOTA-TATE and compared it to untreated mice with HCT116/SSTR2 tumors. Surprisingly the PET imaging suggested that the recurrent tumors no longer expressed SSTR2 (Supplementary Fig S7). The loss of SSTR2 in these tumors was also validated by immunofluorescent staining of tumor sections from mice of both 3.7 MBq

and 7.4 MBq groups (Supplementary Fig. S8). The loss of SSTR2 expression and/or *in vivo* selection of cells that do not express SSTR2 explain the lack of response to the second injection of ^{90}Y -EB-TATE (Fig. 4A). Interestingly, the loss of SSTR2 expression by HCT116/SSTR2 tumors occurred over 2 weeks (Supplementary Fig. S9).

In a subsequent therapy study using high SSTR2 expression model, AR42J xenografts, we observed complete regression of the SSTR2⁺ tumors and full survival for the mice treated with one dose of 3.7 MBq or 7.4 MBq ^{90}Y -EB-TATE. A single dose of 7.4 MBq ^{90}Y -TATE was completely effective ($p < 0.001$, Figs. 4C and 4D).

Staining for markers of tumor cell proliferation (Ki-67) and DNA damage/ cell apoptosis (TUNEL) showed that mice that received 7.4 MBq had significantly lower Ki-67 positive levels and higher TUNEL signal than the other groups (Fig. 5). H&E staining for the tumors revealed extensive necrotic areas for the 7.4 MBq ^{90}Y -EB-TATE HCT116/SSTR2 treated group (Fig. 5).

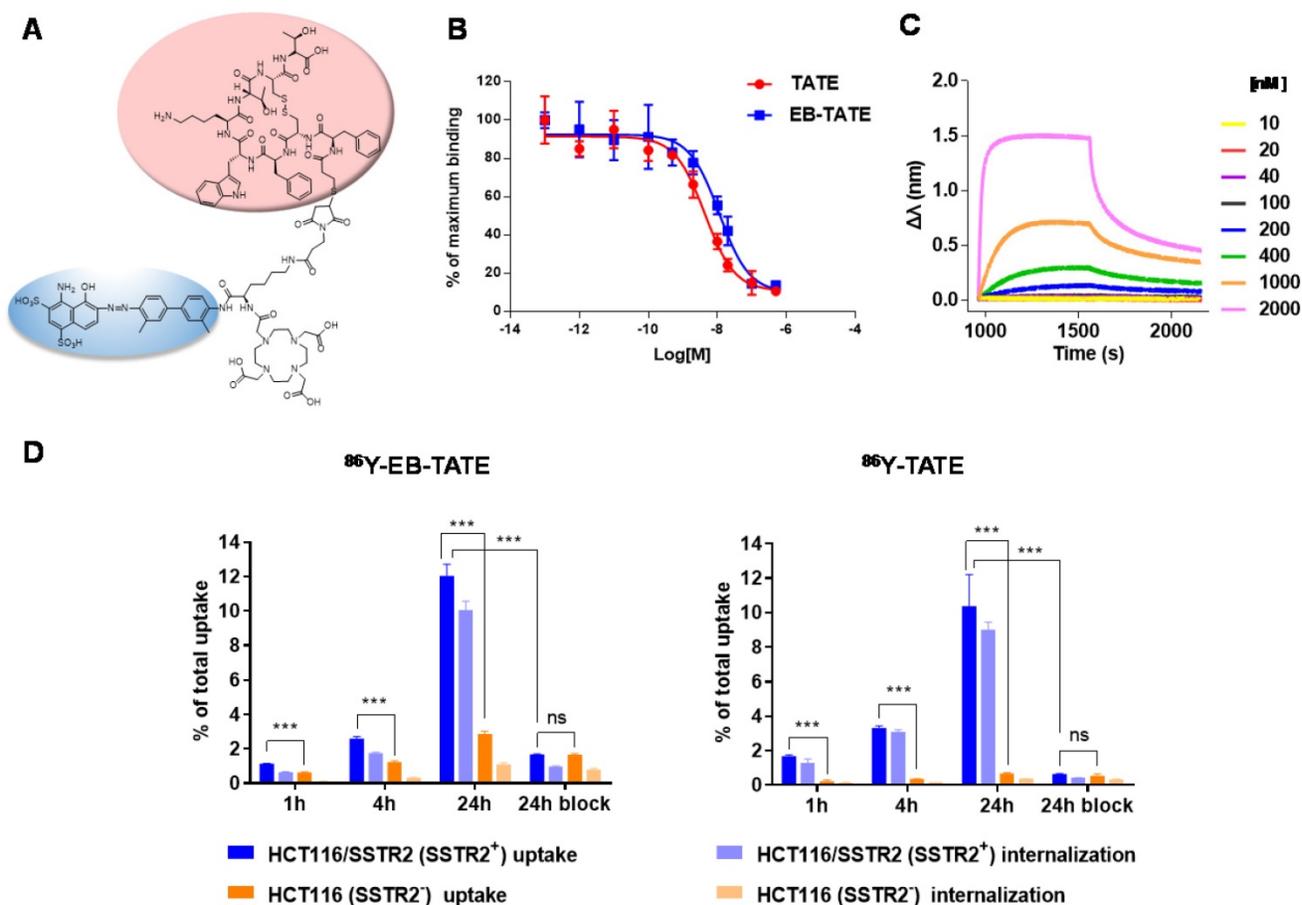


Figure 2. *In vitro* characterization of EB-TATE. (A) Chemical structure of EB-TATE. Truncated Evans blue, which binds to serum albumin, is marked in blue circle. The SSTR2-specific TATE peptide is shown in a pink circle. (B) Cell binding affinity assays of TATE vs. EB-TATE in HCT116/SSTR2 cells. IC_{50} of TATE (red curve): 10.21 ± 1.42 nM, and IC_{50} of EB-TATE (blue curve): 16.50 ± 1.36 nM. Results are shown as average \pm SD of triplicates. (C) Kinetic binding assay of EB-TATE to albumin measured by biolayer interferometry. EB-TATE-albumin complex had a K_{on} of 58233, K_{off} of 0.2843 and a K_D of 4.8 μM . (D) Uptake and internalization in HCT116/SSTR2 (SSTR2⁺) and HCT116 (SSTR2⁻) of ^{86}Y -EB-TATE and ^{86}Y -TATE in the presence of 1% (w/v) of human serum albumin. Blocking studies were evaluated at 24 h. Results are shown as average \pm SD of triplicates. *** $P < 0.001$.

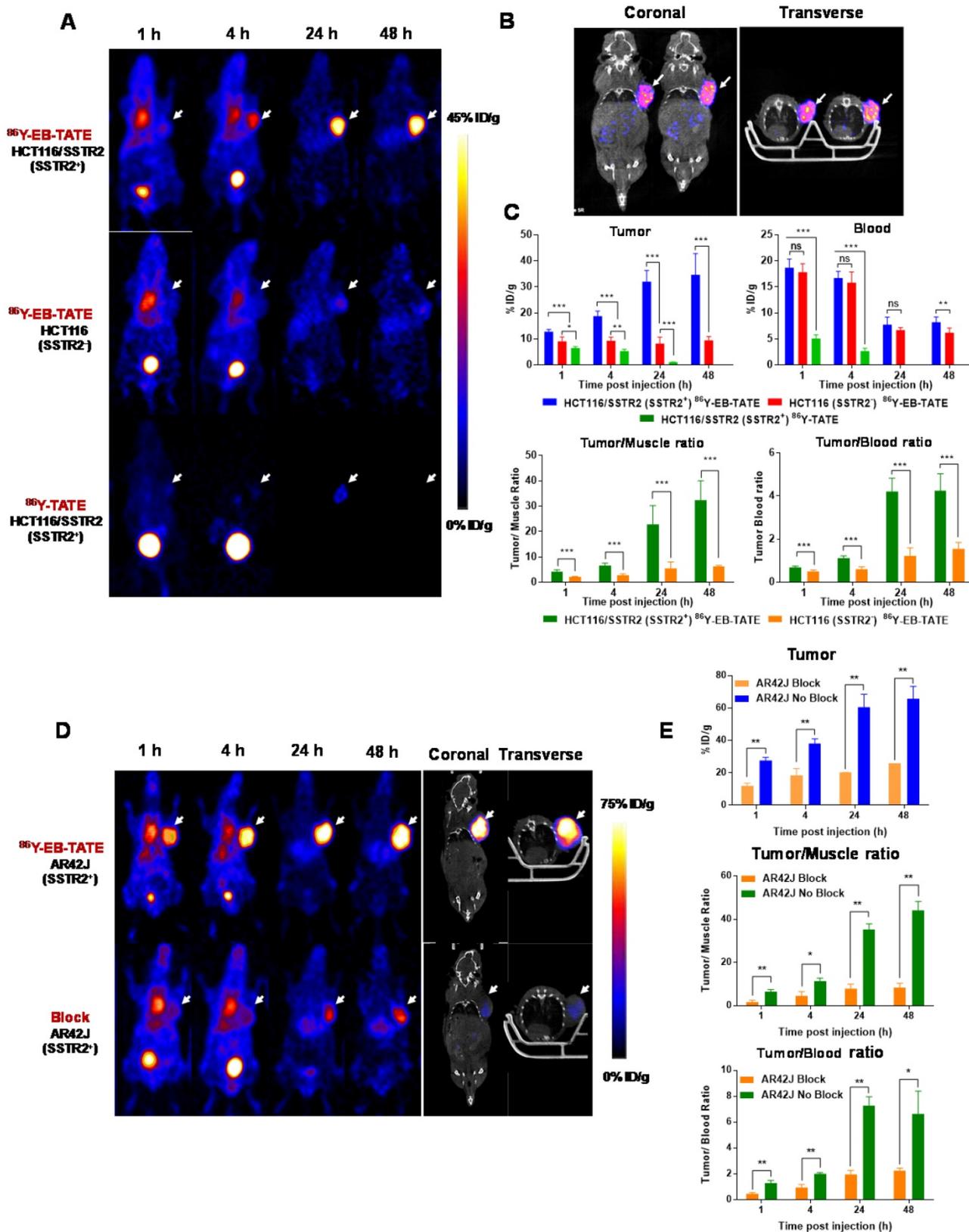


Figure 3. *In vivo* distribution of EB-TATE. (A) Representative projection PET of HCT116/SSTR2 (SSTR2⁺) and HCT116 (SSTR2⁻) tumor models, injected with ⁸⁶Y-EB-TATE or ⁸⁶Y-TATE over time. (B) Co-registration of coronal PET/CT of HCT116/SSTR2 injected with ⁸⁶Y-EB-TATE at 24 h p.i. White arrows indicate the tumor location. (C) Quantification of %ID/g of indicated tracer in tumor and blood (left) and tumor-to-muscle and tumor-to-blood ratios calculated from PET over time in HCT116/SSTR2 tumor model. (D) Representative projection PET (left) and PET/CT (right) of AR42J (SSTR2⁺) xenografts injected with ⁸⁶Y-EB-TATE (upper panel) or ⁸⁶Y-EB-TATE co-injected with unlabeled EB-TATE (>50 fold excess) for blocking. (E) Quantification of %ID/g of indicated tracer in tumor, and tumor-to-muscle and tumor-to-blood ratios calculated from PET over time in AR42J tumor model. White arrows indicate the tumor location. ***P* < 0.01, ****P* < 0.001.

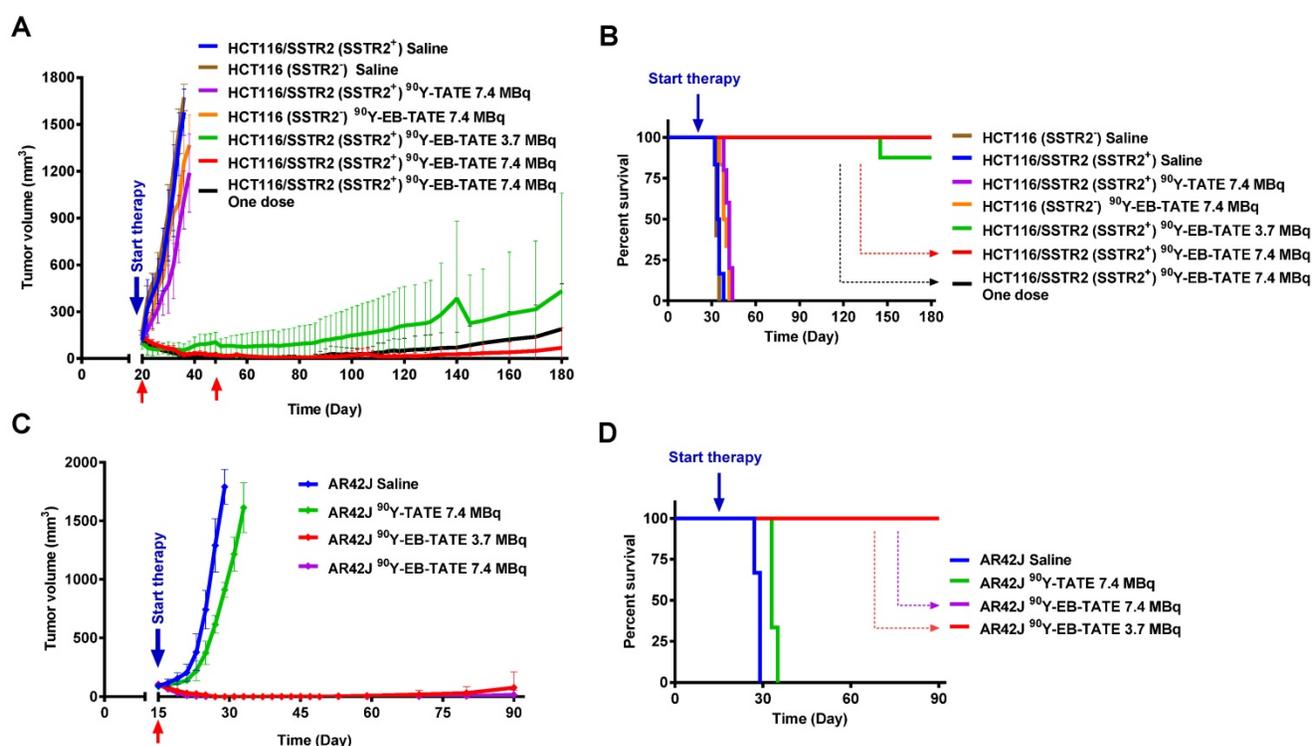


Figure 4. Radionuclide tumor therapy using ⁹⁰Y. (A) Tumor volume (mm³) of mice bearing HCT116/SSTR2 or HCT116 tumors, injected with either saline, 7.4 MBq ⁹⁰Y-TATE, 7.4 MBq ⁹⁰Y-EB-TATE (one or two doses) or 3.7 MBq ⁹⁰Y-EB-TATE. Red arrows indicate day of injection of the radionuclide to the corresponding group. (B) Survival analysis of mice after radiotherapy study described in A. (C) Tumor volume (mm³) of mice bearing AR42J tumors, injected with either saline, 7.4 MBq ⁹⁰Y-TATE, 7.4 MBq ⁹⁰Y-EB-TATE or 3.7 MBq ⁹⁰Y-EB-TATE. Red arrows indicate day of injection of the radionuclide to the corresponding group. (D) Survival analysis of mice after radiotherapy study described in C. *P* < 0.001 for ⁹⁰Y-EB-TATE groups (3.7 and 7.4 MBq) compared to all other groups at all time points.

To test for possible systemic toxicity of the radiotherapy, the body weight of all the mice was monitored throughout the radiotherapy studies (Supplementary Figs. S10 and S11). Although mice treated with 3.7 MBq and 7.4 MBq ⁹⁰Y-EB-TATE showed slight weight loss, they quickly regained the weight back to normal levels. In accordance, pathologic examination of H&E staining of selected non-cancerous organs and blood analysis revealed no obvious differences between the groups (Supplementary Fig. S12-S13 and Table 1). Biodistribution studies of ⁹⁰Y-EB-TATE, using a lower dose of 1.85 MBq, was conducted to observe longer term radioactivity uptake (Supplementary Fig. S14). Unexpectedly, at such a low dose, ⁹⁰Y-EB-TATE still had significant radiotherapeutic efficacy on SSTR2⁺ tumors, and the tumors were significantly smaller at day 4 post-injection. As a result, the amount of radioactivity in the tumor was significantly reduced (Supplementary Fig. S14). To ensure that the radioactivity accumulation in the tumor was not due to transchelation, the tumors were extracted at days 1, 4, 7 and 12 post-injection and evaluated by radioTLC, which indicated no "free" ⁹⁰Y form in the tumor (Supplementary Fig. S15).

Discussion

Optimal pharmacokinetics is the Achilles' heel of many drugs, imaging tracers, and radiotherapeutic agents. We recently reported the development of EB-RGD tracer that provided improved pharmacokinetics compared to RGD, and was successfully used as imaging tracer and radiotherapy agent in mouse tumor models (18). Here, we applied the same strategy to improve the pharmacokinetics of TATE peptide, which is a radiotherapeutic agent employed in the clinic. TATE PRRT against somatostatin receptors (SSTRs) has revealed significant potential for the treatment of advanced, low- to intermediate-grade NETs (17). ¹⁷⁷Lu-DOTA-TATE is currently the most widely used SST analog in the clinic (17). Nevertheless, its efficacy is limited to about 30% overall response rate despite administration of the high cumulative activity of 29 GBq (17). We hypothesized that improvement of pharmacokinetics of radioactive TATE derivatives would improve tumor uptake, increase treatment efficacy, and, because of reduced renal excretion, reduce the radiation exposure to the kidneys.

Our strategy to improve TATE pharmacokinetics was to synthesize an analog with affinity for human serum albumin, which would be expected to decrease

its clearance rate. Human serum albumin, the most abundant protein in blood plasma (~ 50 mg/ml), is the chief carrier protein in the blood and has been exploited as a drug carrier since the mid-1990s (20,21).

In the present study, we designed a new molecule, EB-TATE, by conjugation of TATE with an analog of the azo dye, Evans blue (EB) (Fig. 3). Evans blue and its analogs exhibit modest affinity for serum albumin.

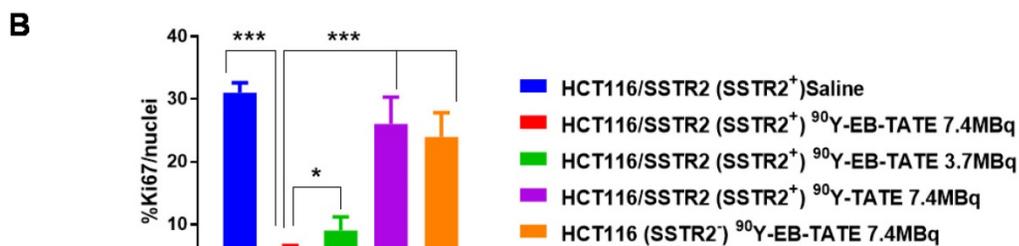
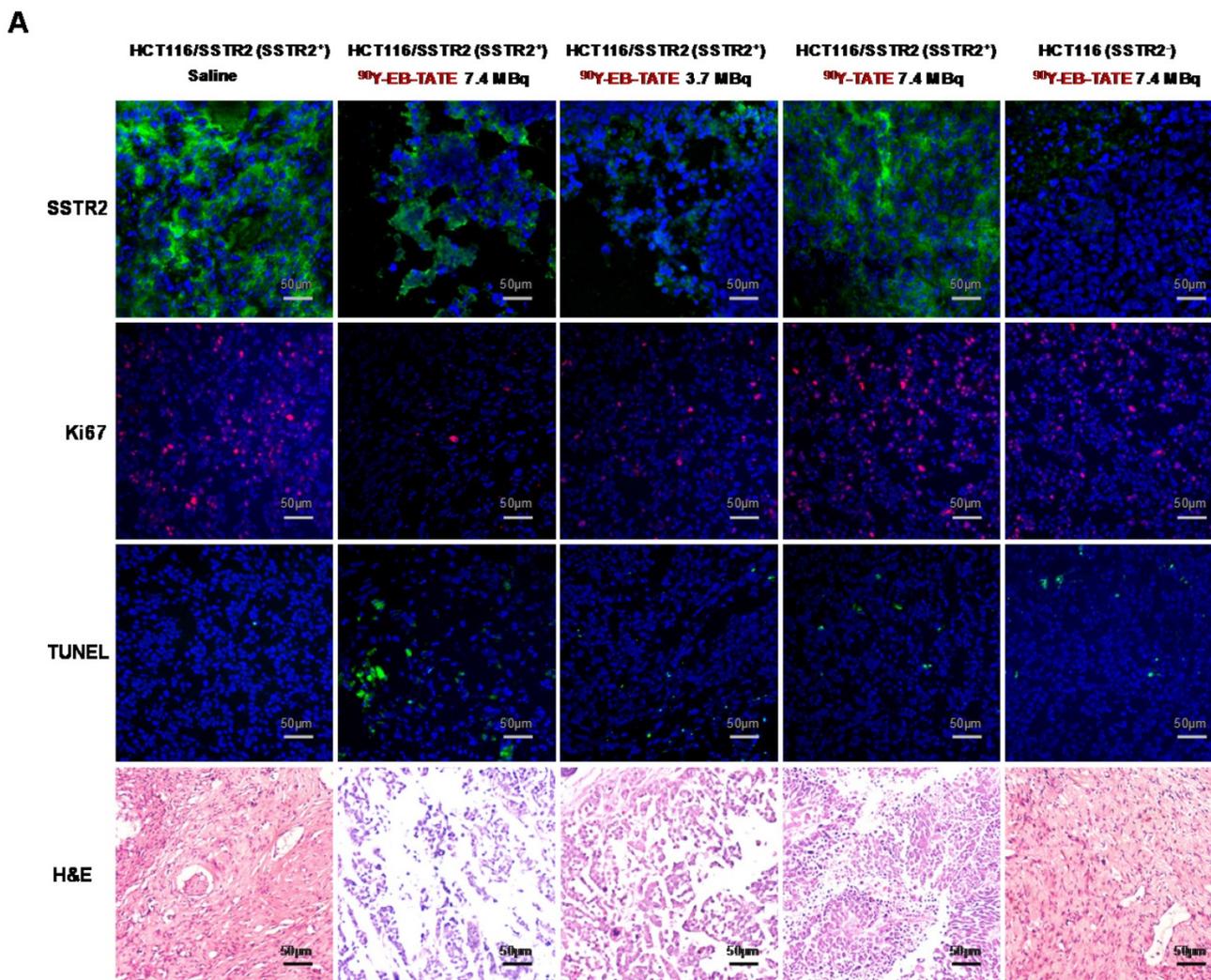


Figure 5. (A) Tumor biology evaluation after ⁹⁰Y radiotherapy. Immunofluorescence staining (X20) of excised HCT116/SSTR2 tumors for SSTR2 levels (green), Ki-67 (red), TUNEL (green) and H&E after radiotherapy treatment was terminated. In all immunofluorescent staining, blue is nuclear staining. (B) Mean percentage of cells stained for Ki-67 quantified from immunofluorescence staining of excised HCT116/SSTR2 tumors; Saline (blue bar 31 ± 1.6), 7.4 MBq ⁹⁰Y-EB-TATE (red bar 4 ± 2.6), 3.7 MBq ⁹⁰Y-EB-TATE (green bar 9 ± 2.2), 7.4 MBq ⁹⁰Y-TATE (purple bar 26 ± 4.3) and excised HCT116 tumors (orange bar 24 ± 3.8). * *P* < 0.05, *** *P* < 0.001.

Table 1. Complete blood counts from mice injected with 7.4 MBq ^{90}Y -EB-TATE (treated) and saline (control) at 90-120 days post-injection.

	Treated		Control		Units
	Average	STD	Average	STD	
WBC count	2.7	0.8	2.8	0.8	K/ μL
RBC count	7.7	0.8	8.3	0.3	M/ μL
Hemoglobin	12.6	1.0	14.3	0.9	g/dL
Hematocrit	40.5	3.7	43.8	2.1	%
MCV	53.0	1.2	53.2	1.8	fL
Platelets	955.5	189.1	934.5	149.7	K/ μL
Polys	24.0	7.9	21.8	2.8	%
Lymphocytes	57.3	11.7	64.6	4.1	%
Polys Absolute	0.7	0.4	0.7	0.3	K/ μL
Lymphocytes Absolute	1.37	0.40	1.81	0.50	K/ μL

During circulation, EB-TATE will be in equilibrium binding with serum albumin. EB-TATE released from albumin in the vicinity of the higher affinity SSTR2, will bind to the receptor expressing cells and subsequently be internalized. The improved pharmacokinetics of EB-TATE, demonstrated by both longer-half life and higher retention in the blood pool, resulted in significantly higher accumulation of ^{86}Y -EB-TATE in SSTR2⁺ tumor (Fig. 3) and enhanced target to background ratios.

When ^{90}Y was used in place of ^{86}Y , the improved pharmacokinetics provided unparalleled radiotherapy of established SSTR2-positive tumors. AUC calculation comparing ^{86}Y -EB-TATE to ^{86}Y -TATE showed approximately 6-fold higher exposure to the radioisotope (Supplementary Fig. S5.). This difference is a low estimation because ^{90}Y has longer half-life and the decline in activity seen in tumors from mice injected with ^{86}Y -EB-TATE was only due to radioactive decay and not biological clearance. In accordance, in SSTR2 mouse xenografts a single injection of 7.4 MBq was enough to eradicate SSTR2⁺ tumors (Fig. 4), in contrast to the multiple injection employed in the clinic. A rough dosimetry calculation using the NCI recommended formula (22) showed that treatment of a mouse at an average weight of 27 g with 7.4 MBq is equivalent to treatment of a human subject that weighs 60 Kg with 1.3 GBq, which is an order of magnitude lower than the cumulative 29 GBq currently being used in the clinic. Similarly, other published studies with ^{90}Y -labeled modified octreotide (23) also had to use very high dose (370 MBq ^{90}Y - octreotide for a 300 g rat), and only small but not large tumors had favorable response to one cycle of radiotherapy.

Previous studies have reported that the treatment of some SSTR2-positive tumors resulted in loss of receptor expression and regrowth of tumors (1,24). We have witnessed this same result following the sub-optimal therapy dose of 3.7 MBq (Fig. 4A).

The recurring tumors did not respond to additional ^{90}Y -EB-TATE, and showed low uptake of ^{68}Ga -DOTA-TATE on diagnostic imaging. The higher dose of ^{90}Y -EB-TATE, 7.4 MBq, led to eradication of tumors without the emergence of SSTR2-negative tumors thereafter.

In conclusion, we have designed a theranostic agent, based on TATE peptide, that targets SSTR2-expressing tumors and demonstrates improved pharmacokinetics. Utilizing a PET radionuclide, ^{86}Y , and a therapeutic radionuclide, ^{90}Y , we obtain improved contrast for imaging and effective radiotherapy of SSTR2-positive tumors. The results described herein are highly encouraging and suggest that the EB-TATE tracer should be evaluated in human trials.

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- Writing, review and /or revision of the manuscript: Orit Jacobson, Rui Tian, Dale Kiesewetter, Xiaoyuan Chen
- Administrative, technical, or material support: Gang Liu, Guizhi Zhu, Ying Ma
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Supplementary Material

Supplementary figures.

<http://www.thno.org/v08p0735s1.pdf>

Competing Interests

The authors have declared that no competing interest exists.

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